

## Flow field-flow fractionation for the characterization of lipid-based colloidal formulations

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### Outline

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#### *Asymmetrical flow field-flow fractionation* (AF4)

principle

separation channel

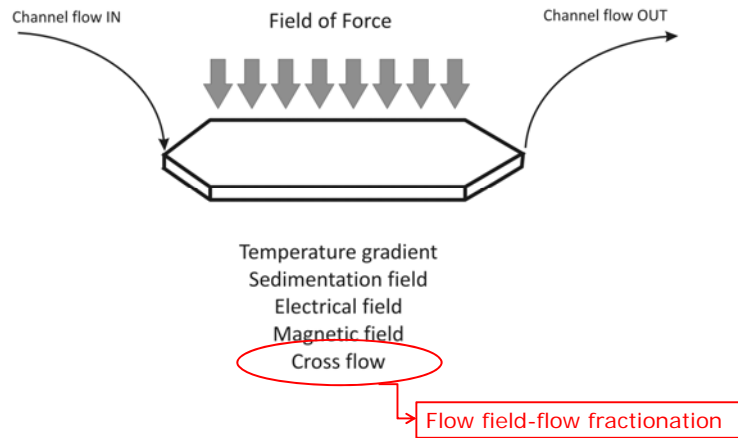
promises of AF4 for the characterization of colloidal  
formulations

#### *Multi-angle laser light scattering* (MALLS) for size determination

#### *Selected results* of current projects

1. drug release and transfer of a water-insoluble model  
drug from liposomes
2. Evaluation of the effect of autoclaving on poloxamer-  
stabilized trimyristin dispersions

## Field-flow fractionation

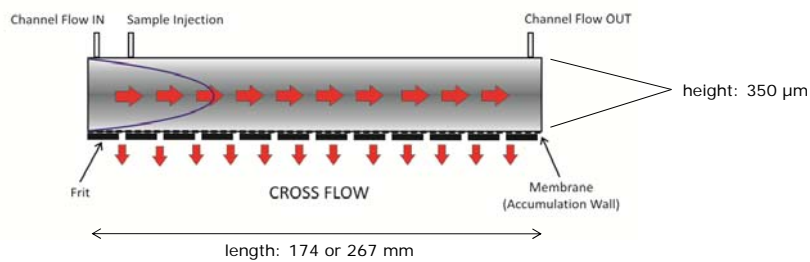


*Cölfen & Antonietti, Adv. Polymer Sci. 150 (2000).*

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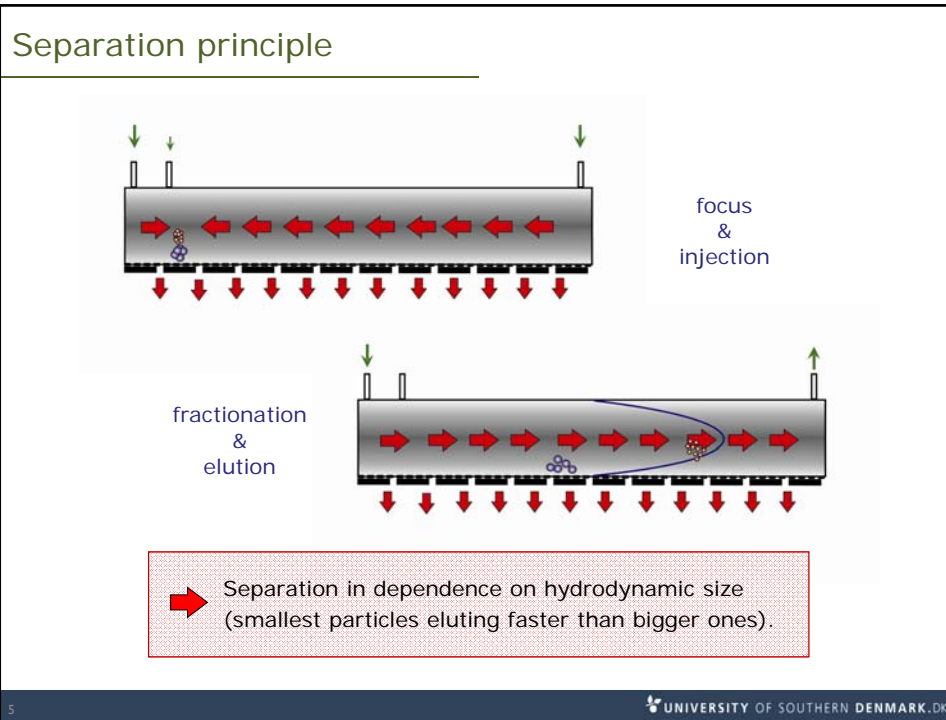
## Asymmetrical flow field-flow fractionation (AF4)



- ← closed cover plate
- ← spacer  
→ defines channel geometry (trapezoidal)
- ← membrane (accumulation wall)  
→ usually PES or RC with MWCO 5-10 kDa

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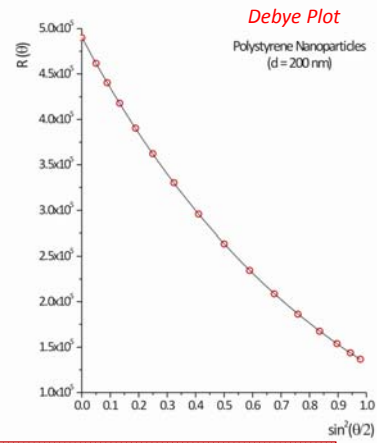
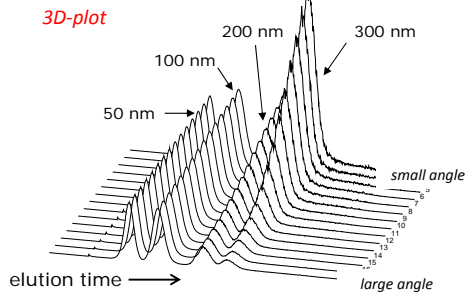


- ### Promises of AF4 for the characterization of nano-sized drug carriers
- broad separation range (~ 5/10 kDa - ~ 1  $\mu\text{m}$ )
  - large variability in flow conditions, channel geometries, solvents, ...
  - accurate size determinations due to separation prior size determination
  - overall gentle separation and no stationary phase
  - semi-preparative fractionation
  - connection with various detectors:
    - multi-angle light scattering (MALLS) (size)
    - refractive index (concentration of dissolved compounds)
    - absorbance (scattering effects needs to be taken into account when measuring particulate formulations)
    - others: fluorescence, MS, ...
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## Size determination by MALLS

### Multi-angle laser light scattering (MALLS)

Polystyrene nanoparticle mixture  
( $d = 50, 100, 200$  and  $300$  nm)



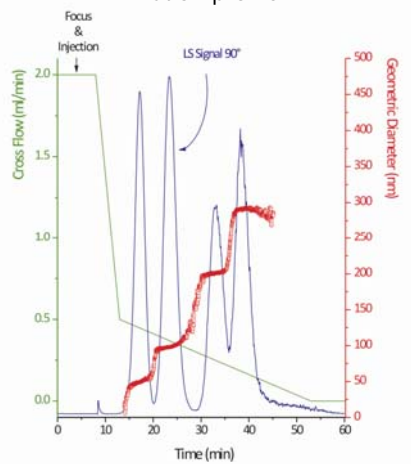
➔ Due to sample fractionation prior size determination (MALLS), accurate information about size distributions is obtained.

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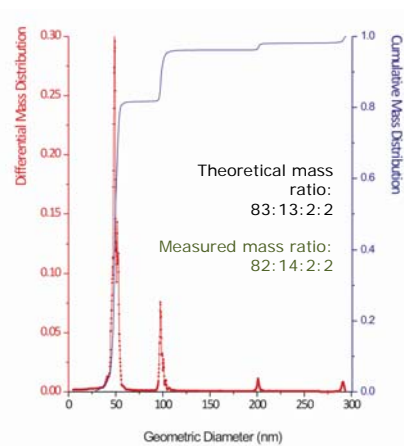
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## Size determination (mixture of PS nanospheres)

### Elution profile



### Size distribution



Kuntsche et al., *J. Biomed. Nanotechnol.* 5 (2009).

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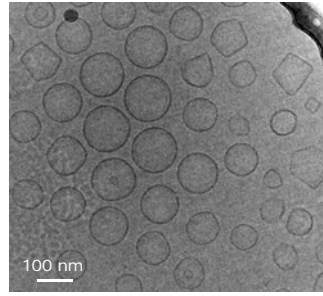
## Example 1: Studies on drug release and transfer

After intravenous injection of a **drug carrier** formulation (liposomes, lipid nanoparticles), the drug may (depending on its physicochemical properties on carrier properties):

- be release into the aqueous phase of blood (molecularly dissolved)
- transfer to other colloidal components of the blood (e.g. lipoproteins, albumin)
- transfer to membranes (e.g. erythrocytes)



challenge in the development of liposomes & lipid nanoparticles for lipophilic drugs

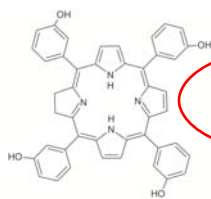


cryo-TEM of mTHPC-loaded liposomes

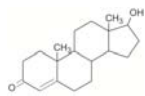
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## Lipid and drug recovery after AF4

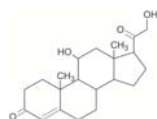
Radioactively labeled liposomes (lipid and drug,  $^3\text{H}$  and  $^{14}\text{C}$ )  
(20 mg/ml DPPC/DPPG loaded with 8 mol% drug, diameter ~ 110-120 nm)



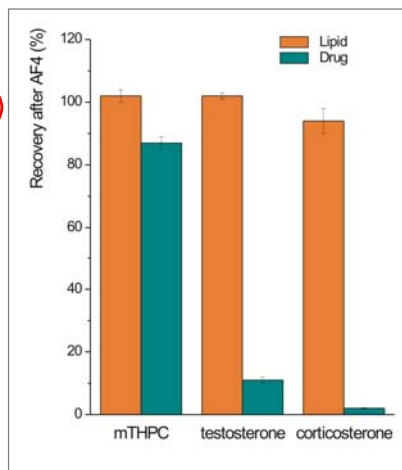
temoporfin (mTHPC)  
(log P ~ 9)



testosterone  
(log P ~ 3)



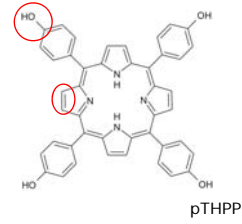
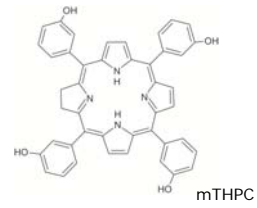
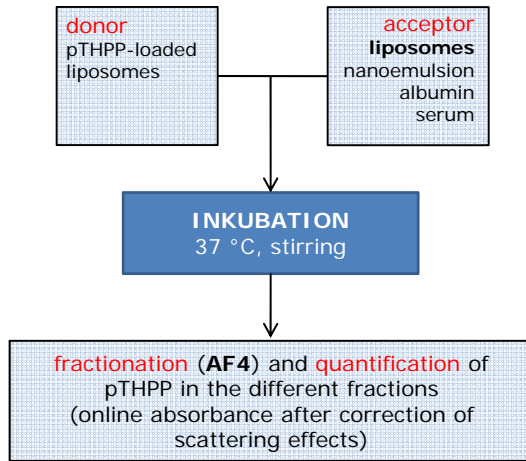
corticosterone  
(log P ~ 2)



Kuntsche et al., *J. Sep. Sci.* 35 (2012).

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## Transfer studies

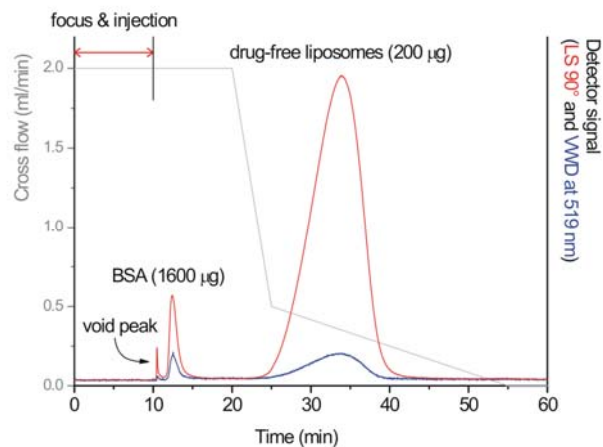


**Prerequisite:** No (or only very minor) overlap of size distributions of the donor and acceptor particles!

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## Separation of liposomes and BSA

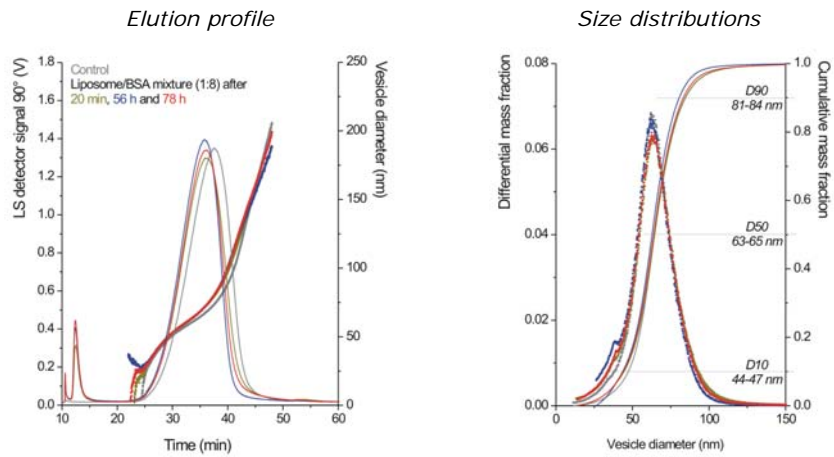


Mixture of liposomes ( $d \sim 65$  nm) and bovine serum albumin ( $d \sim 6$  nm)

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## Liposome size stability during incubation



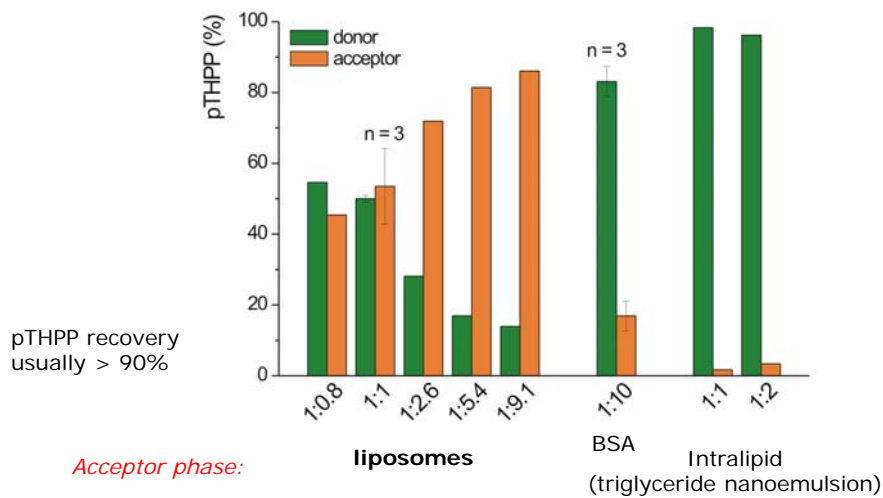
➔ Changes (i.e. in size) in the fractions can be monitored, but (minor) alterations in composition may not be detected

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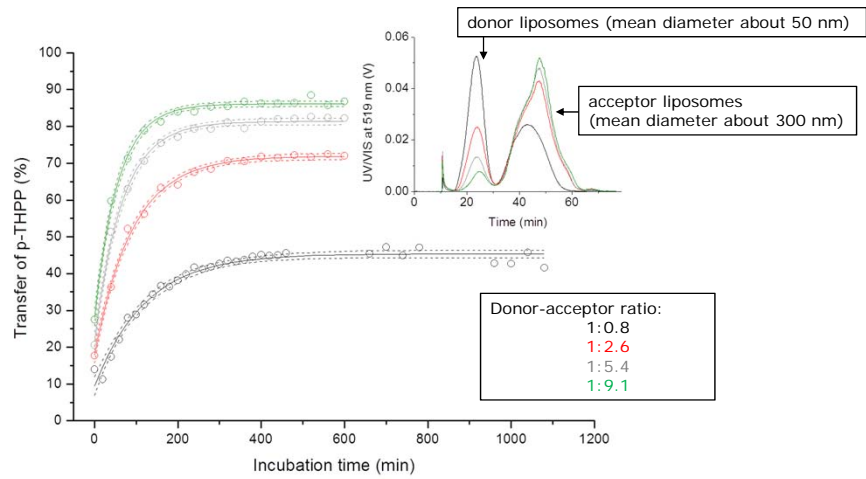
## Extent of pTHPP transfer

pTHPP amount in the **donor** and **acceptor** phase (*in equilibrium*)



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## Transfer kinetics of pTHPP between liposomes



Hinna et al., *Analy. Bioanal. Chem.* 406 (2014);  
 Hinna et al., *J. Pharm. Biomed. Anal.* 124 (2016); Hinna et al., *J. Control. Rel.*, submitted.

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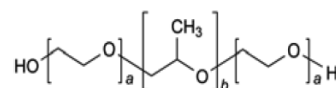
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## Example 2: Effect of autoclaving on poloxamer-stabilized trimyristin dispersions

### Composition

- 10% w/w lipid phase (trimyristin)
- 5 or 12% w/w stabilizer (poloxamer 188)
- water phase with 2.25% w/w glycerol and 0.05% w/w sodium azide

### poloxamer 188 (Ph.Eur.)

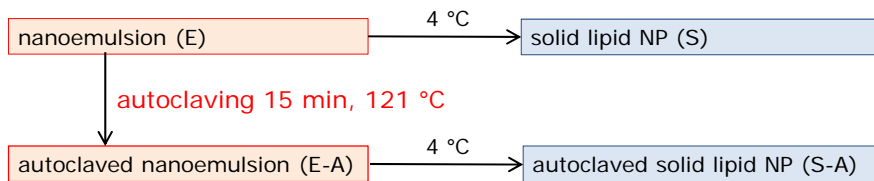


$$a = 75-85, b = 25-30$$

$$\text{average Mw} = 7.68-9.51 \text{ kDa}$$

$$\text{cloud point} > 100 \text{ }^\circ\text{C}$$

### High-pressure melt homogenization (75 °C, different pressures)

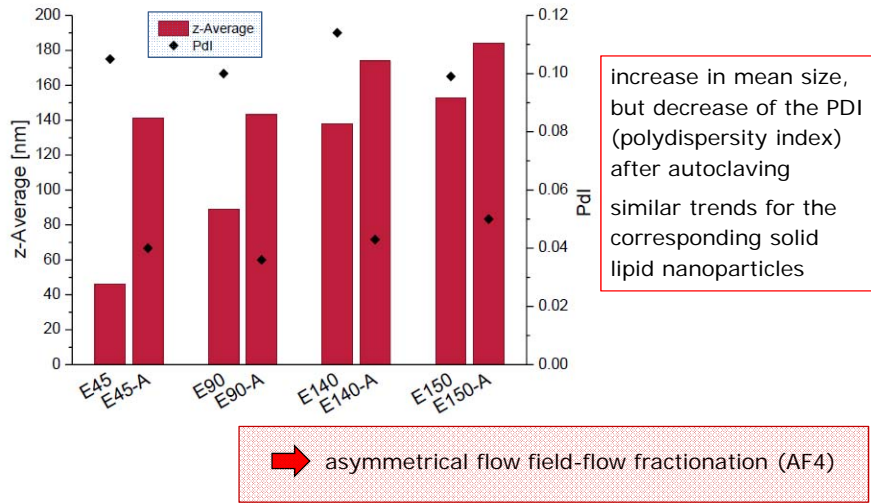


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## Effect of autoclaving on poloxamer-stabilized trimyrustin dispersions

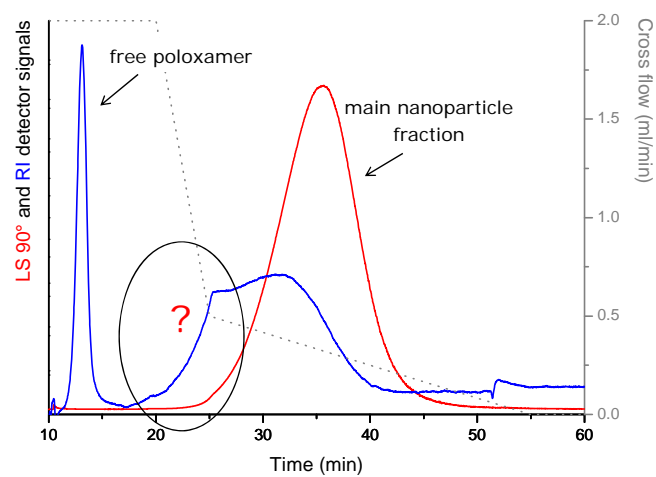


Rose et al., Poster presentation, 9<sup>th</sup> PBP World Meeting, Lisbon, 2014.

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## Elution profile: Non-autoclaved nanoemulsion

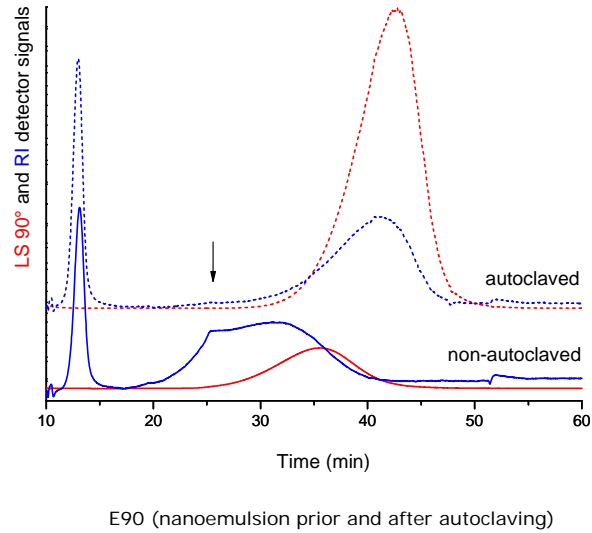


E90 (nanoemulsion prior autoclaving)

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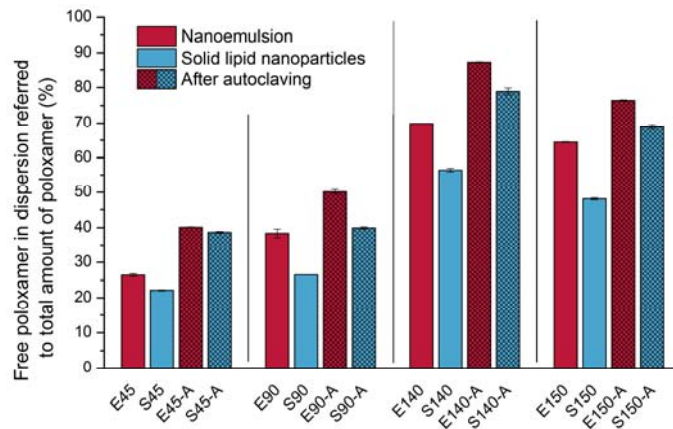
## Elution profile: Effect of autoclaving



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## Amount of free poloxamer in the dispersions



Lower amount of free poloxamer in the solid lipid nanoparticle dispersions and increased amount of free poloxamer after autoclaving.

**Poster 01**

Arnold et al., Poster presentation, 9<sup>th</sup> PBP World Meeting, Lisbon, 2014.

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## Summary and outlook

- AF4 presents a valuable tool for the characterization of colloidal formulations as it facilitates separation of even complex samples.
- *Advantages:*
  - broad separation range over the whole colloidal size range
  - robust and reproducible separations
  - no stationary phase and overall gentle separation conditions
  - monitoring of changes in size during in drug transfer studies
- *Disadvantages/challenges:*
  - requirements on sample (size in the nm-range, physical stability)
  - relatively time-consuming (normally ~ between 45 and 70 min)
  - potential sample-membrane interactions and artifacts due to sample dilution
  - method development may be challenging and time-consuming

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